

"Design and Development of combine bio adhesive – Floating drug delivery system by using different Polymer"

Mr. A. M. Kasambe¹ Mr. N. Kayande²

Department of Pharmaceutics Sunrise University Alwar (Rajasthan) India. Department of Pharmaceutics Sunrise University Alwar (Rajasthan) India.

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ABSTRACT:-The goal of designing sustained release drug delivery systems of tablets is to reduce the frequency of dosing or to increase the effectiveness of the drug by localization at the site of action, reducing the dose required, or providing controlled drug delivery.

The oral route is considered as the most promising route of drug delivery. Effective oral drug delivery may depend upon the factor such as gastric emptying process, gastrointestinal transit time of dosage form. Most of the oral dosage forms possess several physiological limitations such as variable gastrointestinal transit, because of variable gastric emptying leading to non-uniform absorption profiles, incomplete drug release and shorter residence time of the dosage form in the stomach. This lead to incomplete absorption of drug having absorption window especially upper part of small intestine, as once the drug passes down the absorption site the remaining quantity goes down unabsorbed.

KEYWORDS:-Ciprofloxacin HCL55-56, HYDROXYPROPYLMETHYLCELLULOSE

I. INTRODUCTION:-

The gastric emptying time of dosage form in humans is affected by several factors because of which wide inter and intra subject variation are observed hence many drugs are well absorbed in the upper part of the gastrointestinal tract such a high variability may lead to non-uniform absorption and make the bioavailability unpredictable. Hence the beneficial delivery system would be one which possesses the ability to control and prolong the gastric emptying time and can deliver the drug in the optimum concentration to the absorption site (i.e. upper part of small intestine)2.

Gastric emptying of dosage form is extremely variable process and ability to prolong and control the emptying time is valuable asset for dosage forms, which reside in the stomach for a

_____ long period of time than conventional dosage forms. Several difficulties are faced in designing controlled released system for better absorption and enhancement of bioavailability. Conventional oral dosage forms such as tablets, capsules provide specific drug concentration in circulation without offering any control over drug delivery and also cause great fluctuation in plasma drug level. Although single unit floating dosage forms have been extensively studied, these single unit dosage forms have the disadvantage of release all or nothing emptying process while the multiple unit dosage forms along the Gastrointestinal Tract (GIT) could result in more reproducible drug absorption and reduced risk of local irritation; this gave birth to oral controlled drug delivery and led to development of Gastro-retentive Bioadhesive-Floating tablet3, 4.



Figure1: Drug absorption in the case of (a) A Conventional dosage form and (b) In GRDDS

Over the three decade, various attempts have been done to remain the dosage form in the stomach as away increasing retention time .Highdensity system having density 3g/cm3 are retained in the stomach. The only major drawbacks with such system are that it is technically difficult to manufacture them with a large amount of drug (>50%) and to achieve the required density of 2.4-2.8g/cm3. Swelling system are capable of swelling to a size that prevent their passage through the pylorus, the dosage form is retained in the stomach



for a longer period of time. Upon coming in contact with gastric fluid, the polymer imbibes water and swells .Bio/mucoadhesive system bind to gastric epithelial cell surface, or mucin, and extend the Gastro- Retentive time (GRT) by increasing the intimacy and duration of contact between the dosage form and biological membrane.

1.9.1 ADVANTAGES

- Floating system has low bulk density so that they can float on the gastric juice in the stomach. The problem arises when the stomach is completely emptied of gastric fluid.
- In such a situation, there is nothing to float on. But this can be overcome by using bioadhesive -floating drug delivery system.
- In the case of bioadhesive formulation, gastrointestinal motility may be a dislocating force for the dosage form or permanent renewal of the mucus may become an essential limiting factor and specific pH may not be adequate for creating sufficient adhesiveness. But this can be overcome by using bioadhesive- floating drug delivery system.

1.9.2 **DISADVANTAGE**

- There are certain situation where gastric is not desirable. Aspirin and non- steroidal antiinflammatory drug known to cause gastric lesions and slow release of such drug in the stomach is unwanted.
- Thus, drug that may irritate the stomach lining or are unstable in its acidic environment should not be formulated in gastro retentive system.

1.9.3 Drug Suitable For Bioadhesive-Floating Drug Delivery System

- i. Drug acting in the stomach
- E.g. Antacid, Antibiotics, Antimicrobials

ii. Drugs those are primarily absorbed in the stomach

E.g. Albuterol, Ciprofloxacin, Acyclovir

iii. Drugs those are poorly soluble at an alkaline pH

E.g. Chlordiazepoxide, Cinnarazine, diltiazem

iv. Drug with a narrow window of absorption E.g. Riboflavin, levodopa

v. Drugs absorbed rapidly form the GI tract E.g. Amoxicillin

vi. Drugs those degrde in the colon

E.g. Captopril, Ranitidine HCl, Metronidazole, Metformin HCl

vii. Drugs having low solubility at high pH values.

E.g. Diazepam, Furosemide, Verapamil HCl

Objectives:

- Objective of present work was to design and develop bioadhesive-floating drug delivery system by using different polymeric systems which got place in the drug delivery research in order of prolonging time of contact in a oral drug administration, so that the drug delivery system can be maintained at an exacting position for prolong duration for local disease treatment and systemic drug bioavailability.
- Also, to fabricate such controlled bioadhesive drug delivery systems which can offer the advantages of better therapeutic efficacy and is easier to comply with than the conventional regimens requiring more frequent dosing and minimize side effects.

II. DRUG AND EXCIPIENTS PROFILE Structure formula

Ciprofloxacin HCL55-56 HYDROXYPROPYLMETHYLCELLULOSE 57



2.1 CARBOPOL ⁵⁸ SODIUMCARBOXYMETHYLCELLUOSE





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III. EXPERIMENTAL WORK

3.1. Preformulationstudy⁶⁵⁻⁶⁰

Preformulation can be defined asinvestigation of physical

and chemical properties of drugs ubstance alone and wh encombined with excipients. Preformulation studies ar ethe first step in the rational development of dosage form of a drugs ubstance. The objectives of preformulations t udies are to develop aport folio of

informationaboutthedrugsubstance, so that this inform ation is useful to develop formulation. Preformulation investigations are designed to identify those physicochemical properties and excipients that may inf luence the formulation design, methodof manufacture, and pharmacok in etic-

biopharmaceuticalproperties of the resulting product. The goals of the program therefore are:

□ To establish the necessary physicochemical characteristics of a new drugsubstance.

Todetermineitskineticreleaserateprofile.

□ Toestablishitscompatibilitywithdifferentex cipients.

Hence, a preformulation study on the obtained sample of drug includes physical test determination and compatibility studies.

3.2. Characterizationofciprofloxacinhydroc hloride

3.2.1 Organolepticproperties⁶⁷

Thedrugpowderwasanalysedforcolour, odor and taste

3.2.2 Description⁶⁷

Thedrugsample(ciprofloxacinhydrochloride)wasana lysedforphysicalappearanceandpowdernature.

3.2.3 Meltingpoint⁶⁷

Meltingpoint determination of ciproflox a cinhydrochl oridewasdone by open capillary method. It is a good first indication of purity of samples ince

thepresenceofrelativelysmallamount ofimpuritycanbedetectedbyaloweringaswell aswideningofmeltingpointrange.

3.2.4 Solubilityanalysis⁶⁷

A semi quantitative determination of solubility can be made

byaddingasoluteinsmallincrementalamounttofixedv olumeofsolvents, distilled water, phosphate buffer pН 1.2, 7.4. buffer pН 0.1N HCl, methanol, alcohol, isopropylalcohol. After each additi on,thesystemisvigorouslyshaken and examined usually for any undissolve particles. When some soluteremains undissolved the total amount added that point to servers as up а goodandrapidestimateofsolid.

3.3. MicromeriticcharacterizationofCiproflo xacinhydrochloride

IntheMicromeriticproperties,Angleofrepose,looseb ulkdensity, Tapped bulk densities, Carr's index, Hausner ratio of the pure drugweredetermined.Methodsforthe determinationofAngle of repose,Loosebulkdensity,Tappedbulkdensity,Carr's index,andHausnerratio.

3.4. Spectroscopicstudies ⁶⁸

3.4.1 UVspectroscopy(Determinationoflambda max)

Stocksolution($100\mu g/ml$)ofciprofloxacinhydrochlor idewasprepared in 0.1M HCl. The solution was kept in a fused silica cuvette 10mm.The UV spectrum was recorded in the range of 254-365nm on Shimazdu UV-visible spectrophotometer (UV-1700) at 1cm, slit width. The same procedurewascarriedoutusing0.1MHCl.Itshowedma xat275nmusingspectrophotometer.

3.5. CompatibilitystudiesofCiprofloxacinhy drochlorideandformulationcomponents

The compatibility of drug and polymer under experime ntal conditions is important prerequisite before formula tion. It is therefore necessary to confirm that the drug doe snot react with the polymer and excipients under experimental conditions and not affecting the shelf life

ofproductoranyotherunwantedeffectsontheformulati on.

3.6 MicromeriticCharacterizationofDrugandpol ymer⁷¹⁻⁷²

3.6.1 EvaluationofpreparedPowdermixtures 3.6.1.1 LoosebulkDensity

Theloosebulkdensitywasobtainedbydividingthemas sofpowderbythebulkvolumeincm³.The10gmsample wascarefullyintroducedintoa25mlgraduatedcylinder .Thevolumeoccupiedbythepowder was recorded



and bulk density then calculated. It was calculated by using equation given below: $D_f = M/Vp$

3.6.1.2 Tappedbulkdensity:

The tapped bulk density was obtained by dividing the mass of apowderbythetappedvolumeincm³.The10gmsample wascarefullyintroduced into a 25ml graduated cylinder. The cylinder was dropped at 2-second intervals onto a hard wood surface 100 times from a height of 1 inch.

Compressibility Index and Hausner ratio:

In recent years, the compressibility index and the closely related Hausner ratio have become the simple, fast and popular methods of predicting powder flow characteristics.

Hausner Ratio

Flow property	Hausner Ratio
Excellent	1.00-1.11
Good	1.12-1.18
Fair	1.19-1.25
Passable	1.26-1.34
Poor	1.35-1.45
Very poor	1.46-1.59
Very, very poor	>1.60
	Flow property Excellent Good Fair Passable Poor Very poor Very, very poor

Table No.1: Relationship between Percent compressibility And Flowabilit

Table No. 2: Relationship between angle of (θ) and flow ability

Flow Property	Angle of Repose (degrees)
Excellent	25-30
Good	31-35
Fair—aid not needed	36-40
Passable—may hang up	41-45
Poor-must agitate, vibrate	46-55
Very poor	56-65
Very, very poor	>66

Formulation and preparation of floating-Bio adhesive tablets of Ciprofloxacin HCl

Sustained release floating- Bio adhesive tablets were prepared by direct compression method. Ciprofloxacin and various concentrations

HPMC K- 15M were used as a release retardant polymer. Carbopol -940, Sodium CMC and Sodium alginate were used as bio adhesive polymer. Sodium bicarbonate.



Batches/Ing	drug	HPMCK.	Carbopo	1 SodiumC	SodiumA	1 Sodiumbic	a £ itrica	c MCC	Total(
redients		15	940	MC	ginate	onate	iđ		mg)
(mg)									
F1	500	125	25	-	25	25	25	25	750
F2	500	100	50	-	25	25	25	25	750
F3	500	75	75	-	25	25	25	25	750
F4	500	125	-	25	25	25	25	25	750
F5	500	100	-	50	25	25	25	25	750
F6	500	75	-	75	25	25	25	25	750
F7	500	100	25	25	25	25	25	25	750
F8	500	125	12.5	12.5	25	25	25	25	750
F9	500	150	-	-	25	25	25	25	750

Table no. 3: Formulation Chart of bio adhesive-floating tablet of ciprofloxacin

Evaluation of Ciprofloxacin bioadhesive-floating tablets Weight variation test ^{65, 66, 71, 72}

Weighing 20 tablets individually, calculating the

average weight and comparing the individual tablet weight to the average USP weight variation test. The table No4 given below shows the weight variation tolerance for uncoated tablets.

Table No.04: Weight variation tolerance for uncoated tablets				
Average weight of Tablet (mg)	Maximum percent deviation allowed			
80mg or less	10%			
80mg to 250mg	7.5%			
More than 250mg	5%			

Hardness

The hardness of 3 tablets, from each batch was determined and means hardness was taken into account, which was expressed in kg/cm2.

Friability

Friability test is performed to assess the effect of friction and shocks, which may often cause tablet to chip, cap or break. Roche friabilator was used for the purpose. Tablets were deducted and re-weighed. Compressed tablets should not loose more than 1% of their weight.

Content uniformity

For this at least 30 tablets were randomly selected. Out of 30 tablets, 10 tablets were crushed into fine powder and assayed individually; the

tablet should be within 85% to 115% of the labeled claim.

Thickness

The thickness of the tablet was measured using Verniercalliper. Thickness of three tablets from each batch was measured and mean was calculated.

Swelling characteristics of tablet

The extent of swelling was measured in term of percent weight gain by the tablets. The swelling behaviour of formulation was studied. One tablet from each formulation was kept in Petri dish containing for 0.1N HCl 12 hours. At the end of each hour tablet was withdrawn soaked with tissue paper and weighed. Then after every hrs.



Swelling index of tablet was calculated using formula.

Determination of floating capacity In vitro bio adhesion study.

Bio adhesive strengths of the tablets were measured on a modified physical balance

(Figure.no.13). The apparatus consist of a modified double beam physical balance in which a right and left pans has been replaced by lighter pans. The left side of the balance was made 5gm heavier than the right side by placing 5gm weight on left side pan



Figure 02: Bio adhesion Test study assembly

Table No.05: Parameters of dissolution studi

Speedofrotation	50rpm
No.oftabletstested	6tablets
Temperature	37°C±0.5°C
Time	24hours
TestMedium	0.1NHCL
Volumeoftestmedium	900mlineachvesselfor24hrs.
Samplingtime	Eachtwohours

EffectofdrugreleaseinintestinalpHcondition^{85,86,a} nd87

Model fitting ^{88, 89,90,91,92}

The model fitting for % cumulative release was done using PCP software to find the best fits kinetic equation for the dissolution profile

Kinetics of drug release

In order to understand the mechanism and kinetics of drug release, the results of the in-vitro dissolution study of the optimized batch was fitted with various kinetic equations like. Zero order (% Release =Kt), First order (log % Unreleased =Kt), Higuchi's model (% Release =Kt0.5) and Pappas Korsmeyer equation (% Release=Ktn)



Parameters				
	Atinitial	After 1month	After2month	After3month
Thickness	5.67±0.0 08	5.67±0.0 08	5.67±0.00 8	5.67±0.0 08
Hardness	5.3±0.4	5.2±0.4	5.3±0.4	5.3±0.4
Drugcontent	98.31%	98.28%	98.22%	98.15%

Stability studies of ciprofloxacin hydrochloride matrix tablets TableNo.06:ParametersstudiedonF2,formulationsbeforeandafterstability study

TableNo.07:%CumulativePercentdrugreleasedofoptimizedformulationF2,after stabilitystudy

%cumulative			
Atinitial	After 1month	After2month	After3month
0	0	0	0
15.61	15.61	15.61	15.61
22.98	22.58	22.92	22.76
32.94	31.94	31.85	32.48
47.04	46.04	44.16	46.92
52.40	50.87	51.27	52.25
61.30	58.37	59.30	60.85
64.04	63.21	62.66	63.95
73.75	70.87	71.85	72.25
78.77	76.15	75.35	74.50
87.96	84.36	83.67	86.58
94.81	92.32	93.68	93.35
98.19	97.45	99.67	97.95
	%cumulative Atinitial 0 15.61 22.98 32.94 47.04 52.40 61.30 64.04 73.75 78.77 87.96 94.81 98.19	%cumulative drug release Atinitial After 1month 0 0 15.61 15.61 22.98 22.58 32.94 31.94 47.04 46.04 52.40 50.87 61.30 58.37 64.04 63.21 73.75 70.87 78.77 76.15 87.96 84.36 94.81 92.32 98.19 97.45	%cumulative drug release Atinitial After 1month After2month 0 0 0 0 15.61 15.61 15.61 15.61 22.98 22.58 22.92 32.94 31.94 31.85 47.04 46.04 44.16 52.40 50.87 51.27 61.30 58.37 59.30 64.04 63.21 62.66 73.75 70.87 71.85 78.77 76.15 75.35 87.96 84.36 83.67 94.81 92.32 93.68 98.19 97.45 99.67

*AllthevaluesarerepresentsasMean±S.D.(standarddeviation)(n=3)





Figure.03: Dissolution profile of formulations F2 before and after stability study

	Swellingstu			
Time(hr)	Atinitial	After 1month	After 2month	After3mont h
1	33.33	31.65	32.12	33.19
2	36.25	32.35	34.57	33.58
4	65.10	62.57	61.79	64.84
6	78.20	74.69	76.15	77.23
8	103.28	100.25	102.89	102.89
10	120.22	118.69	120.12	119.46
12	97.38	96.89	101.21	98.08

Table no.08: Swelling index of F2 formulation before and after stability study

Figure.04: Swelling index of formulations F2 before and after stability



Table 09: Floating capacity of F2 formulation before and after stability study

	Floatingcapacity			
Time(hr)	Floatinglagtime(sec)	Totalfloatingtime		
Atinitial	20	Morethan12hr.		
After 1 Month	24	Morethan12hr.		
After 2	21	Morethan12hr.		



month		
After 3	22	Morethan12hr.

Table 10: Invitrobio adhesion study of F2 formulation before and after stability

		In vitrobioadhesion study			
Time(hr)		Bioadhesive Strength(gm)	Bioadhesive Force(N)		
Atinitial		19.38	0.1935		
After 1 Month	L	19.34	0.1932		
After 2 month	2	19.37	0.1931		
After 3 month	}	19.36	0.1934		

Figure.05:InvitrobioadhesionstudyofformulationsF2beforeandafterstability



IV. SUMMARY AND CONCLUSION

Main challenge to controlled/sustained release drug delivery system is to uphold the drug delivery system at exacting site for extensive time period for local and systemic bioavailability of drug also these system has disadvantage of less gastric retention time, which is a physiological limitation that leads to lower bioavailability of drug. Mostly, for a conventional dosage form the dosing intervals of the drug are much less than the drug half-life leads to numerous limitations. The remedy for above problems is the development of controlled and targeted drug delivery system of existing drugs which are effective and safe. Therefore bioadhesive-floating dosage form has been selected which remained intact at an exacting site for extensive time period to provide a longer residence time and prolonged release of drug.

Future scope

Itcanbeusedtostudythetargetorientedreleaseofdr uginthecureof diseaserelatedtostomach.



- Developmentof dosage form by using various bioadhesivepolymers.
- Development ofbioadhesivestrengthstudymodel.
- Invitrogastroretentivegammascintigraphystudyofpresentwork.
- Studytheeffectoftabletshapeandsizeonthechara cteristicsofsuchdosageform.
- Invitro-invivocorrelationofpresentstudy.

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